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**Relationships between hippocampal atrophy, white matter disruption and grey matter
hypometabolism in Alzheimer's disease**

Running Head: Hippocampal disconnection and hypometabolism in AD

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Abstract

In early Alzheimer's disease (AD), the hippocampal region is the area most severely affected by cellular and structural alterations, yet glucose hypometabolism predominates in the posterior association cortex and posterior cingulate gyrus. One prevalent hypothesis to account for this discrepancy is that posterior cingulate hypometabolism results from disconnection from the hippocampus through disruption of the cingulum bundle. However, only partial and indirect evidence currently supports this hypothesis. Thus, using structural MRI and ^{18}F FDG-PET in 18 patients with early AD, we assessed the relationships between hippocampal atrophy, white matter integrity and grey matter metabolism by means of a whole brain voxel-based correlative approach. We found that hippocampal atrophy is specifically related to cingulum bundle disruption, which is in turn highly correlated to hypometabolism of the posterior cingulate cortex but also of the middle cingulate gyrus, thalamus and mammillary bodies (all part of Papez' circuit), as well as the right temporo-parietal associative cortex. These results provide the first direct evidence supporting the disconnection hypothesis as a major factor contributing to the early posterior hypometabolism in AD. Disruption of the cingulum bundle also appears to relate to hypometabolism in a large connected network over and above the posterior cingulate cortex, encompassing the whole memory circuit of Papez (consistent with the key location of this white matter tract within this loop) and also, but indirectly, the right posterior association cortex.

Introduction

Prototypical brain glucose metabolism alterations in patients with Alzheimer's disease (AD), also observed in patients with amnesic Mild Cognitive Impairment (MCI), are characterized by early involvement of the posterior cingulate cortex (PCC), subsequently spreading to the neighboring precuneus and temporo-parietal neocortical areas (Chételat et al., 2003b;Mevel et al., 2007;Nestor et al., 2004).

There is a striking discrepancy between this hypometabolic profile and the well-described pattern of grey matter (GM) atrophy mainly affecting first the medial and then the lateral temporal areas, before extending to the cingulate cortex and temporo-parietal regions (Chételat et al., 2003a;Matsuda et al., 2002;Thompson et al., 2003;Whitwell et al., 2007), consistent with the course of neurofibrillary degenerations in AD (Braak and Braak, 1991). The most robust and widely held hypothesis to account for this discrepancy is that the hypometabolism of the posterior association cortex and more particularly the PCC does not only result from local neuropathological processes, but largely reflects the distant effect of neuronal damage in the hippocampal formation (including the hippocampus proper and the parahippocampal cortex), i.e. a disconnection process (Chételat et al., 2003a;Jobst et al., 1992;Matsuda et al., 2002;Meguro et al., 2001;Nestor et al., 2003;Nestor et al., 2004;Smith, 2002).

There is long-standing evidence for this “diaschisis” hypothesis from neuropathological studies. Hyman *et al.* (1984) first pointed out the specific alteration of hippocampal and parahippocampal neurons involved in connecting the hippocampal formation with other brain structures. Subsequently, Pearson *et al.* (1985) hypothesized a mechanism of neuropathological alterations expansion in AD along the projecting fibers, notably hippocampal projection neurons. And Jobst *et al.* (1992) first postulated a distant

effect of the hippocampal region atrophy to explain the reduced blood flow in the posterior areas.

This diaschisis hypothesis has since been repeatedly mentioned, and further supported by indirect or partial evidence. For instance, PCC hypometabolism was observed in non-human primates following hippocampal and parahippocampal lesions (Machado et al., 2008; Meguro et al., 1999). In addition, significant positive correlations were reported in patients with AD between hippocampal formation size on the one hand, and either PCC activation during a memory task (Garrido et al., 2002; Remy et al., 2005), or posterior associative cortical areas resting-state metabolism (Meguro et al., 2001). Recent studies using diffusion tensor imaging (DTI) in AD have documented disruption of the cingulum bundle (Fellgiebel et al., 2005; Rose et al., 2000; Teipel et al., 2007; Zhang et al., 2007), a white matter (WM) tract linking the hippocampus proper and parahippocampal cortex to the PCC (Mori et al., 2005; Morris et al., 1999; Mufson and Pandya, 1984; Schmahmann and Pandya, 2006), as well as its relationship with global and hippocampal atrophy (Firbank et al., 2007; Xie et al., 2005).

Although the above findings argue in favor of a disconnection hypothesis to explain PCC hypometabolism in early AD, there is to date no direct evidence that PCC hypometabolism results from hippocampal formation atrophy *via* cingulum bundle disruption. The aim of the present study is to further explore this hypothesis by assessing the relationships between hippocampal atrophy, WM integrity and GM metabolism in patients with clinically probable AD.

Subjects and Methods

Subjects

Eighteen patients were studied, all right-handed with at least 8 years of education. At the time of the study, none of the patients was being or had been treated with specific medication, such as anti-acetylcholinesterasic drugs. All were prospectively selected using standard NINCDS-ADRDA diagnostic criteria for probable AD (McKhann et al., 1984), based on an extensive neuropsychological examination as detailed elsewhere (Baron et al., 2001;Chételat et al., 2008;Desgranges et al., 1998). Only patients who had both T1-weighted magnetic resonance imaging (MRI) and positron emission tomography (PET) coupled to [^{18}F]-2-fluoro-2-deoxy-D-glucose (^{18}FDG) examinations and MMSE>20 (i.e. mild AD) were included in the present study. Fifteen unmedicated healthy controls who also underwent both MRI and PET were also studied, all right-handed with at least 8 years of education. They were screened for the absence of cerebrovascular risk factors, mental disorder, substance abuse, head trauma and significant MRI or biological abnormality. The two groups were matched for age, and although women were over-represented in the AD sample compared to controls, this difference was not significant (χ^2 Yates correction=2.21; $p=0.13$) (see **Table 1** for demographic data). The subjects were the same as those studied in Chételat *et al.* (2008). All the subjects were fully cooperative and free from behavioral disturbances. They all gave their consent to the study after detailed information was provided to them and the PET procedure was approved by the Ethical Committee of the University of Caen. The study was done in line with the Declaration of Helsinki.

Imaging data acquisition

For each subject, a high-resolution T1-MRI scan was obtained, which consisted in a set of 128 adjacent axial slices parallel to the anterior commissure-posterior commissure (AC-PC) line with slice thickness 1.5 mm and pixel size $0.9375 \times 0.9375 \text{ mm}^2$ using the spoiled gradient

echo sequence (SPGR) (repetition time (TR)=10.3 ms; echo time (TE)=2.1 ms; field of view (FoV)=240x180 mm²; matrix=256x192). All the MRI data sets were acquired on the same scanner (1.5 T Signa Advantage echospeed; General Electric, Milwaukee, WI).

Each subject also underwent a PET study within days of the MRI study. Data were collected using the Siemens ECAT Exact HR+ PET device with isotropic resolution of 4.6×4.2×4.2 mm³ (axial FoV= 158 mm). The patients had been fasting for at least 4 hours before scanning. To minimize anxiety, the PET procedure was explained in detail beforehand. The head was positioned on a head-rest according to the cantho-meatal line and gently restrained with straps. ¹⁸FDG uptake was measured in the resting condition, with eyes closed, in a quiet and dark environment. A catheter was introduced in a vein of the arm to inject the radiotracer. Following ⁶⁸Ga transmission scans, three to five mCi of ¹⁸FDG were injected as a bolus at time 0, and a 10 min PET data acquisition started at 50 min post-injection period. Sixty-three planes were acquired with septa out (3D acquisition), using a voxel size of 2.2×2.2×2.43 mm³ (x y z).

Imaging data handling and transformation

The procedure used for data handling and transformation was based on Chételat *et al.* (2008), but WM MRI data were also used for the purpose of the present study and specific GM and WM masks were created. The statistical analyses performed here (see below) were also strictly different.

MRI data

The MRI data sets were analyzed using Statistical Parametric Mapping (SPM2; <http://www.fil.ion.ucl.ac.uk/spm>) and the optimized voxel-based morphometry (VBM) procedure described in detail elsewhere (Good et al., 2001) and already used in our laboratory

(Chételat et al., 2002;Chételat et al., 2005). Briefly, the procedure included the creation of customized templates of the whole brain and the GM, WM and cerebrospinal fluid (CSF) sets using the MRI data from the whole combined patient and control samples (n=33). The original MRI data sets were then segmented into SPM (implying a reversible affine normalization step) using these customized templates as priors. The resultant original (i.e. in native space) GM data sets were then spatially normalized onto the GM customized priors respectively to determine the optimal normalization parameters, which were then applied to the corresponding original whole brain MRI scans. Finally, the “optimally” normalized whole brain MRI data sets were segmented into SPM and the resultant GM and WM partitions were smoothed (14.6 mm full width at half maximum - FWHM; see below) and masked (see below).

PET data

The PET data were first corrected for partial volume effect (PVE) due to both CSF and WM using the optimal voxel-by-voxel method originally proposed by Müller-Gartner *et al.* (1992), and slightly modified as proposed by Rousset *et al.* (1998). This method, referred to as ‘modified Müller-Gartner’, is described in details in Quarantelli *et al.* (2004), and has already been applied in our laboratory (Chételat et al., 2003b;Chételat et al., 2008;Mevel et al., 2007). All image processing steps for PVE correction were carried out using the ‘PVE-lab’ software (Quarantelli et al., 2004). Using SPM2, PVE-corrected PET data sets were then coregistered onto their respective MRI and spatially normalized onto the same GM customized template as that used for the spatial normalization of MRI data, by reapplying the normalization parameters estimated from the VBM procedure. The normalized PET data sets were then smoothed (14 mm FWHM; see below). The resulting PET images were divided by their individual vermis FDG uptake value to control for individual variations in global PET

measures, following the procedure already used in our laboratory (see Mevel *et al.*, (2007) for details). Smoothed and scaled PET data were then masked using the same GM mask as that used for the GM partition obtained from MRI data (see below).

Differential smoothing

To blur individual variations in gyral anatomy and increase the signal-to-noise ratio, the spatially normalized GM and WM partitions and the corrected and spatially normalized PET data sets were smoothed. We used the standard Gaussian kernel of 14 mm FWHM for the PET data. Since PET and MRI data had different original spatial resolutions, differential smoothing was applied in order to obtain images of equivalent effective smoothness, and thus of identical resultant resolution (Richardson *et al.*, 1997; Van Laere and Dierckx, 2001). To this end, we used a Gaussian kernel of 14.6 mm FWHM for the MRI GM and WM data, resulting in an effective smoothness identical to PET images smoothed at 14 mm FWHM (Poline *et al.*, 1995).

Masking

The GM, WM and PET images obtained following the steps above were masked so as to include only GM or WM voxels of interest and to prevent any overlap between voxels included in analyses with GM and those with WM. The GM mask was obtained by first thresholding the GM customized template above a value of 0.3, corresponding to a higher than 30 percent chance for the voxel to belong to GM. The resultant “permissive” GM mask was then manually adjusted in order to exclude any voxel of WM (such as the interfaces between CSF and WM misclassified as GM: fornix, ventricles edges, ...). A WM mask was then obtained by first creating a “permissive” WM mask by thresholding the WM customized template above a value of 0.15, excluding the pons and cerebellum and then excluding all

voxels included in the final GM mask. The same binary GM mask was applied to both the GM and the PET data sets and binary WM mask was applied to the WM data set.

Z-score maps

The smoothed and masked GM, WM and PET images were used to create Z-score maps ([patient individual value - controls mean] / controls standard deviation), for each patient and each modality. The GM, WM, and PET Z-score maps thus obtained for each patient were then entered in the correlative analyses described below.

Statistical analysis

WM atrophy

Since the profiles of GM atrophy and hypometabolism have been described elsewhere (Chételat et al., 2008), only the pattern of WM atrophy will be detailed here. Group differences were assessed to obtain maps of statistically significant WM atrophy in AD patients relative to controls, using the smoothed and masked WM data set obtained as described above and the two-sample t-test SPM2 routine.

Correlation between atrophied hippocampal formation GM Z-score and whole brain WM Z-score maps

The full procedure of data analysis is summarized in **Figure 1**. First, mean hippocampal formation GM Z-scores were extracted from the significantly atrophied hippocampal formation GM voxels (obtained by comparing AD patients with controls using the two-sample t-test SPM2 routine), using a p (False Discovery Rate corrected for multiple comparisons) < .05 threshold with k > 20 voxels (**Figure 1-B**). Since both the parahippocampal gyrus and the hippocampus proper send direct projections *via* the cingulum bundle (and thus

potentially liable to cingulum atrophy), we used the mean GM Z-score (termed “hippocampal formation GM Z-score”) across the significantly atrophied voxels of these two anatomical labels when assessing correlations with WM Z-score maps. Anatomical labeling was based on the Anatomical Automatic Labeling (AAL) software (Tzourio-Mazoyer et al., 2002) after normalization of the anatomically labeled MNI template onto our customized template.

Second, positive correlations were computed across the 18 AD patients between hippocampal formation GM Z-scores and whole brain WM Z-score maps, using the “single-subject: covariates only” SPM2 routine. This procedure allows to perform linear regressions between one or more variables of interest and each voxel of the maps entered into the analysis. Note that we also compared the correlations with GM Z-Scores in the hippocampus proper to that in the parahippocampal gyrus to assess whether these two structures show any significant difference in their relationships with WM atrophy.

Correlation between WM Z-scores and whole brain PET Z-score maps

The mean WM Z-score from the main cluster of the previous correlation analysis (between hippocampal formation GM Z-Scores and WM Z-Score maps) thresholded at p (FDR corrected) $<.05$ with $k>20$ voxels, was extracted for each patient (**Figure 1-D**). These individual values of WM Z-score were then entered as covariates in a statistical analysis of positive correlations with the PET Z-score maps, using the “single-subject: covariates only” SPM2 routine. The resulting SPM-T map was then converted to a R^2 map.

Statistical threshold and display of results

SPM-T maps of all previously described analyses were thresholded using a p (FDR corrected for multiple comparisons) $<.05$ threshold with a $k > 20$ voxels. In order to avoid type II errors due to over-conservative threshold, results were also displayed using a more liberal

uncorrected $p < .05$ threshold with a $k > 20$ voxels. Correlations were only assessed in the physiologically expected (i.e. positive) direction, corresponding to our hypothesis of a relationship between GM atrophy, WM atrophy, and GM hypometabolism (see Introduction). Anatomical localization was based on the superimposition of the SPM-T and R^2 maps onto the customized template, and identification of the localization using the AAL software and anatomical atlases (Mori et al., 2005; Talairach and Tournoux, 1988; Tzourio-Mazoyer et al., 2002). The findings were also rendered using the publicly available "Anatomist/BrainVISA" software (www.brainvisa.info).

Results

The profiles of GM atrophy and hypometabolism, described in detail in Chételat *et al.* (2008), were consistent with the characteristic pattern of brain alterations in AD, mainly involving the hippocampal formation and temporal neocortex for the former (see **Figure 1-A** for an overview of GM atrophy), and posterior associative areas including the PCC for the latter.

WM atrophy

Regions of significant WM atrophy are displayed in **Figure 2**. They included the corpus callosum (CC), fornix, cingulate WM including the cingulum bundle (involving both its rostral and caudal portions), parahippocampal clusters corresponding to the perforant path, and temporal WM clusters (see **Table 2**).

Correlation analysis

Positive correlations between hippocampal formation GM Z-scores and WM Z-score maps are displayed in **Figure 1-C**. Significant correlations were found with the right cingulate WM

including the caudal part of the cingulum bundle, the largest and most significant cluster, but also with frontal and parahippocampal WM clusters mainly corresponding to the rostral and most caudal parts of the cingulum bundle respectively (see **Table 2**, **Figure 1-C**). When lowering the statistical threshold to $p < .05$ uncorrected, the correlation concerned both the left and right cingulum bundles along their whole length, curving around the temporal horns of the lateral ventricles and joining together all the previously described clusters from the frontal to the parahippocampal fibers (see **Figure 3**). The posterior part of the CC (splenium) was also found significantly correlated using this more permissive threshold (see **Figure 3**).

No significant difference (p (FDR corrected for multiple comparisons) $< .05$) was found in the correlations between the WM Z-Scores maps and the GM Z-Scores for the hippocampus proper and the parahippocampal gyrus (data not shown).

Positive correlations between the mean WM Z-scores of the right cingulate WM cluster (centered at 27 -53 31, MNI coordinates, see **Table 2**), corresponding to the main cluster of the previous analysis ($p < .05$ FDR corrected; see **Table 2**), and PET Z-score maps were found in the middle cingulate cortex, the PCC (mostly its retrosplenial part; BA29/30) and precuneus, hippocampal and parahippocampal regions as well as several subcortical structures including the thalamus and the mammillary bodies (see **Table 2**, **Figure 1-E** for whole brain R^2 results and **Figure 4** for the SPM-T map thresholded at p FDR corrected $< .05$). The R^2 maps revealed R^2 values between 0.5 and 0.8 within these clusters (see **Figure 1-E**). A few tiny right temporo-parietal clusters were also found (see **Table 2**), with high R^2 values (0.4-0.5) in the inferior parietal lobule as well as superior, middle and inferior temporal gyri (see **Figure 1-E**). Adding age, MMS score, as covariates showed essentially unchanged partial regressions (data not shown). Note that the same findings were obtained when the cingulum cluster WM Z-scores were derived from a $p < .05$ (uncorrected) threshold, leading to inclusion of the whole bilateral cingulum bundle fibers (data not shown).

Discussion

The present study revealed a pattern of WM atrophy mainly involving the CC, fornix, cingulum, perforant path and temporal WM. There were strong positive correlations between hippocampal formation GM Z-score and WM Z-scores of the cingulum bundle including both its caudal (between the hippocampal formation and the PCC) and rostral (between the PCC and the frontal cortex) parts, and, to a lesser degree, WM Z-score of the splenium. Finally, the cingulum WM Z-score was itself strongly related to PET Z-scores in the posterior and middle cingulate gyri, thalamus, mammillary bodies, parahippocampal cortex, hippocampus, and right temporo-parietal cortex.

The profile of WM atrophy observed in AD in the present study using VBM and showing a major involvement of the cingulum bundle, is highly consistent with our disconnection hypothesis. The involvement of this tract as well as the CC, fornix, perforant path and temporal WM is consistent with previous findings from DTI studies that reported diffusivity increases or anisotropy decreases in the same set of WM areas (Fellgiebel et al., 2004;Huang et al., 2007;Medina et al., 2006;Teipel et al., 2007;Xie et al., 2006;Zhang et al., 2007). Atrophy of the CC and perforant path have also already been highlighted in previous VBM studies of AD (Chaim et al., 2007) and MCI (Stoub et al., 2006), respectively. That highly consistent patterns of WM atrophy are defined using two highly different methods of acquisition and analysis such as DTI and VBM is noteworthy, and our study further emphasizes the validity and sensitivity of automatic whole-brain VBM to assess WM atrophy in AD.

One first main objective with this study was to assess the relationships between hippocampal formation GM atrophy and whole brain WM atrophy. We found a strong and specific correlation of hippocampal formation atrophy with cingulum bundle atrophy, documenting that disruption of the cingulum bundle is specifically related to atrophy of the hippocampal formation. Our findings are consistent with a previous report using DTI that showed a significant correlation between cingulum bundle fractional anisotropy and hippocampal volume (Xie et al., 2005). We also found a weaker correlation with the splenium, likely corresponding to the tapetum, an inter-hemispheric tract located at the posterior-most part of the CC that links both temporal lobes together (Mori et al., 2005;Schmahmann and Pandya, 2006). These results thus suggest that hippocampal formation atrophy may be related to disruption of the connections between the medial temporal lobe and the contro-lateral temporal cortex.

Moreover, these relationships were found to be relatively specific. As both the hippocampal formation and the cingulum bundle were markedly atrophied, this correlation could reflect association rather than causality, i.e. it could be due to an independent effect of AD on these two structures. However, correlations were not found to involve any atrophied WM tract (even when lowering the statistical threshold), but only those known to be connected to the hippocampal formation (see **Figures 1-C** and **4**). Further, there also seems to be some specificity among the hippocampal formation tracts, since for instance the fornix, which is both atrophied and connected to the hippocampus (Duvernoy and Vannson, 1998), did not exhibit a significant correlation. This suggests the involvement of alternative causes for WM tract alteration over and above hippocampal damage, as well as particular vulnerability in AD pathology for those hippocampal neurons that project through the cingulum bundle.

The strongest correlation with hippocampal formation atrophy concerned the caudal part of the cingulum bundle, which mainly includes fibers connecting the parahippocampal gyrus and hippocampus proper to the PCC (Kobayashi and Amaral, 2003;Kobayashi and Amaral, 2007;Mori et al., 2005;Mufson and Pandya, 1984;Schmahmann and Pandya, 2006). Correlations were also found for the rostral part of the cingulum bundle, which notably comprises hippocampo-frontal (Morris et al., 1999;Mufson and Pandya, 1984) and retrosplenial-frontal tracts. It suggests that hippocampal formation atrophy in AD also leads to the disruption of fronto-hippocampal connections, not only directly, but also indirectly through the damaged retrosplenial PCC (BA 29 and 30), since this area “provides the most direct and most massive route for information flow between the dorsolateral frontal cortex and the medial temporal lobe” (Kobayashi and Amaral, 2003; see also Kobayashi and Amaral, 2007;Morris et al., 1999). These hypotheses are further supported by functional connectivity studies showing a decrease in fronto-hippocampal connectivity at rest (Allen et al., 2007;Wang et al., 2006) as well as during a memory task (Grady et al., 2001) in AD.

Our second main objective was to assess the relationships between cingulum bundle atrophy and cortical hypometabolism. The results highlighted strong correlation with posterior cingulate hypometabolism and more specifically its retrosplenial part (see **Figures 1-E** and **4**). This is the first direct evidence relating PCC hypometabolism to hippocampal atrophy *via* the cingulum bundle disruption, further supporting the “diaschisis” hypothesis for PCC hypometabolism in AD. The precise localization of this correlation to the retrosplenium is entirely consistent with the neuroanatomy, since BA29 and 30 are the PCC subregions mainly connected to the hippocampal formation *via* the cingulum bundle (Kobayashi and Amaral, 2003;Kobayashi and Amaral, 2007). The R^2 values for this correlation reached 0.5 to 0.8, i.e. cingulum bundle atrophy explained about 50-80% of PCC metabolism variance independently

of age and MMS score. Thus, neither age nor disease severity, but the loss of hippocampal inputs itself, accounts for the majority of PCC hypometabolism in AD. This is consistent with the fact that the hippocampal-cingulate fibers represent the main input to the retrosplenium (Kobayashi and Amaral, 2003).

Cingulum bundle atrophy was also found to be related to hypometabolism of the mammillary bodies, thalamus, middle cingulate gyrus, parahippocampal gyrus and hippocampus. This finding might reflect the key location of the cingulum bundle within the hippocampo-mammillo-thalamo-cingulo-parahippocampal loop, i.e. the Papez' circuit (Papez, 1937), as it includes connections between the cingulate gyrus and both the thalamus and the parahippocampal gyrus (Mufson and Pandya, 1984). Thus, cingulum bundle atrophy likely disrupts Papez' circuit, leading to hypometabolism affecting its nodes.

Relatively high R^2 values (0.4 to 0.5) also involved the right temporo-parietal cortex. This finding is somewhat unexpected since the temporal neocortex does not receive direct projections from the cingulum bundle (Mori et al., 2005; Mufson and Pandya, 1984; Schmahmann and Pandya, 2006). However, this correlation is weaker than that for the above-mentioned regions directly connected *via* the cingulum, and as such may reflect an indirect relationship. Using a correlative approach in humans, Vogt *et al.* (2006) recently highlighted regions mono- or multi-synaptically linked to the ventral PCC, pointing to a large association temporo-parietal region that encompasses the area found here. Thus, cingulum bundle might induce temporo-parietal hypometabolism through an indirect connection involving the ventral PCC. It is noteworthy that this correlation was found with the right temporo-parietal cortex only. Evidence of asymmetric pathological mechanisms in AD have been frequently documented, notably concerning GM atrophy (Thompson et al., 1998; Thompson et al., 2003) and hypometabolism (Haxby and Rapoport, 1986). Recently,

several studies characterizing the earliest metabolic alterations in AD pointed to the right temporo-parietal areas (Chételat et al., 2003b; Hirao et al., 2005; Ishii et al., 2005; Kawachi et al., 2006). While the lateralization obtained here remains to be elucidated, it might reflect a still unexplained asymmetric mechanism of brain alteration in AD.

Strikingly, we found no significant correlation with the metabolism of other structures known to be connected through the cingulum bundle such as frontal areas. This may be due to the fact that, while hippocampal fibers represent the major input to the retrosplenium, hippocampal inputs to other cortical regions and particularly to anterior frontal areas are much less prominent. Consequently, the influence of cingulum bundle disruption would be expected to be weaker in these anterior regions. This lack of correlation might also in part result from functional compensations, particularly in the prefrontal cortex where such processes have been repeatedly reported in AD (Grady et al., 2003; Remy et al., 2005).

The use of Z-Scores in the correlation analyses in this study was preferred here to account for the multi-modality analysis, but could have induced a bias as by definition Z-Scores depend on standard deviation, which could vary across imaging modalities. However, we repeated the same analyses using GM/WM density and PET maps instead of Z-Score maps and similar results were obtained (data not shown). Another issue relates to anatomical accuracy limitation inherent to voxel-based method implying normalization and smoothing. Consequently, SPM findings can be smeared in space (e.g. the cingulate WM clusters obtained here exceed the expected single-subject cingulum bundle width, so that we cannot exclude the involvement of adjacent non-cingulum WM). Moreover, results in small brain structures such as the fornix and mammillary bodies should be considered with some caution given this methodological limitation.

To sum up, by relating the PCC hypometabolism in AD to hippocampal formation atrophy through disruption of the cingulum bundle, this study provides strong and direct support to diaschisis as the link between these two characteristic alterations of AD. Furthermore, posterior cingulate hypometabolism in AD may result from an early disturbance of fronto-hippocampal communications, and cingulum bundle disruption plays a major role in the dysfunction of the major connection nodes of Papez' circuit.

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Figure legends

Figure 1: Illustration of the different analysis steps and their corresponding findings (all the results are displayed at $p < .05$ FDR corrected with $k > 20$ voxels). First, from the voxels of significant GM atrophy in AD compared to controls (**A**), the mean GM Z-score of the bilateral hippocampal formation was extracted for each subject (**B**), and entered as covariate in a correlative analysis with whole brain WM Z-score maps. The results of this correlative analysis are illustrated (**C**) using the Anatomist 3D render (www.brainvisa.info; superior, right and posterior views) as well as the SPM cross-sectional render centered at 22 -48 20 (x y z; MNI coordinates). The WM mean Z-score in the main cluster of the previous analysis, i.e. the caudal part of the cingulum, was then extracted for each subject (**D**) to be entered as covariate in a correlative analysis with the whole brain PET Z-score maps. The results of this analysis are displayed as R^2 maps onto 3D surface renderings (**E**; www.brainvisa.info). L = left; R = right.

Figure 2: Areas of significant decrease in WM density in patients with Alzheimer's disease compared to controls ($p < .05$ FDR corrected with $k > 20$ voxels) as projected onto sagittal sections (MNI coordinates).

Figure 3: Significant correlations between the GM Z-score of the hippocampal formation and the whole brain WM Z-score maps, thresholded at $p < .05$ uncorrected ($k > 20$) and displayed on Anatomist 3D render (www.brainvisa.info; superior, right and posterior views) as well as onto SPM cross-sectional render centered at -24 -40 30 (x y z; MNI coordinates). L = left; R = right.

Figure 4: Overall display of the main findings from this study as projected onto the same brain views. The significantly atrophied hippocampal formation voxels used to extract mean GM Z-scores for the correlation with WM Z-score maps are represented in red. The cingulum cluster resulting from the previous correlative analysis and used to extract the mean WM Z-Scores subsequently correlated to PET Z-score maps, is shown in blue ($p < .05$ FDR corrected, $k > 20$ voxels). Finally, statistically significant positive correlations between WM Z-scores of the cingulum cluster, extracted from the first correlation, and PET Z-score maps are illustrated in green ($p < .05$ FDR corrected with $k > 20$ voxels). L = left; R = right.

Table 1: Demographic characteristics of subjects.

	Healthy Aged Subjects	Patients with Alzheimer's disease
Number	15	18
Males/Females	7/8	3/15
Age (years)		
mean \pm SD	66.5 \pm 7.3	69.5 \pm 5.2
range	60-84	60-82
MMSE		
mean \pm SD		24.3 \pm 2.6
range		20-29

Table 2: Labelization, Montreal Neurological Institute (MNI) coordinates, cluster size in number of voxels, and T value of the significant peaks for the SPM analyses of i) WM atrophy, ii) Correlation between hippocampal formation GM Z-Scores and whole brain WM Z-Score maps and iii) Correlation between cingulum bundle WM Z-scores and whole brain PET Z-Score maps. L = left; R = right.

Region	Size (voxel)	MNI Coordinates			T
		x	y	z	
WM atrophy					
Corpus Callosum R and L Cingulate White Matter	77730	30	32	18	5.69
L Parahippocampal White Matter	472	-26	-16	-29	4.73
L Frontal White Matter	368	-37	38	8	3.41
R Frontal White Matter	421	17	59	12	3.33
L Temporal White Matter	334	-28	-59	-2	2.90
Correlation between hippocampal formation GM Z-Scores and whole brain WM Z-Score maps					
R Cingulate White Matter	14707	27	-53	31	6.49
L Temporal White Matter	1140	-49	-7	-21	4.89
L Frontal White Matter	608	-21	41	-1	4.76
	177	-43	-1	43	4.24
	74	-48	27	15	4.21
	709	-29	-6	30	4.13
	34	-45	37	-3	3.87
R Temporal White Matter	991	43	4	-26	4.72
	903	44	-43	-11	3.28
R Frontal White Matter	39	20	34	38	4.46

Correlation between cingulum bundle WM Z-Scores and whole brain PET Z-Score maps

R Precuneus	5222	8	-27	28	8.51
R Thalamus					
R Middle Cingulate Gyrus					
R Parahippocampal Gyrus					
R Posterior Cingulate Gyrus					
R Hippocampus					
L Thalamus					
L Middle Cingulate Gyrus					
R and L Mammillary Bodies	148	-1	-4	-14	4.70
R Temporal Pole	314	25	9	-41	4.69
R Parahippocampal Gyrus					
R Superior Temporal Gyrus	33	64	-13	-9	4.30
R Supramarginal Gyrus	24	62	-24	17	4.28